

How To Innovate in CV Technology – TCT AP 2011, Seoul

Evolution of Merilimus Eluting Coronary Stent System MITSU Novel Approaches to DES Creation

Ashok Seth

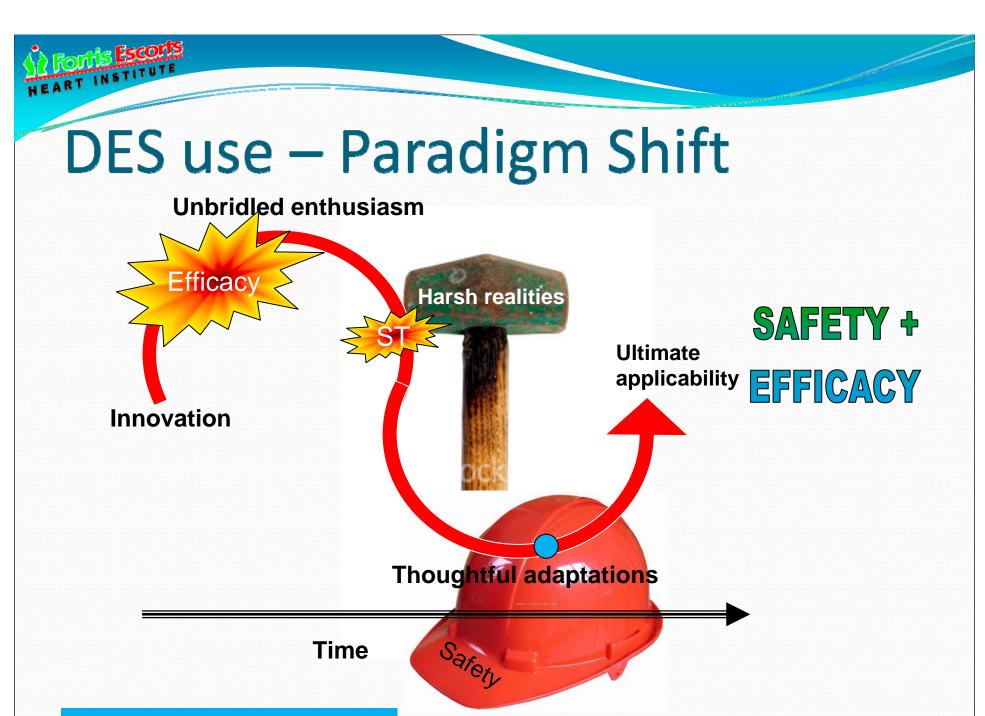
Chairman & Chief Cardiologist
Chairman Cardiology Council, Fortis Group of Hospitals

Fortis Escorts Heart Institute New Delhi



Disclosures

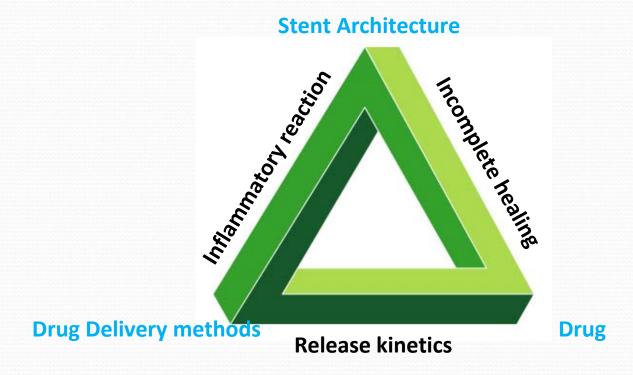
Honorary Advisor to Merill LifeSciences



BioMime/Mitsu entry point



Penrose's Problem in DES Creation



Stent architecture, Polymer and Drug are the most polarized facets in DES construction

Penrose's impossible triangle

DES: A mechanical & pharmacological Approach to CAD. Paul Dobesh et al Pharmacotherapy, 2004



Drivers of DES Safety

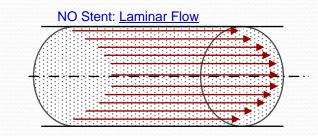
- Acute drivers
 - Vessel injury
 - Complete apposition
 - Biodegradable polymers or no polymers!
 - Premature cessation of antiplatelet Rx
- Long term drivers
 - Re-endothelialisation
 - Functional endothelium
 - No vessel wall inflammation

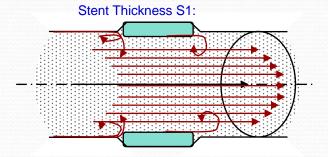


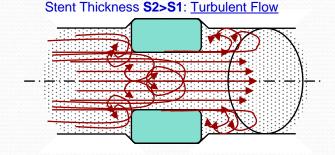
Thin Struts and Restenosis

- Thin Struts allow for-
 - Low blood flow perturbance
 - Easy struts nesting to the vessel wall
 - Added flexibility and conformability
- Improved clinical outcome*
- Improved, faster endothelialization **

- * Kastrati A, Schömig A, Dirschinger J, et al. Strut Thickness Effect on Restenosis Outcome (ISAR STEREO Trial). Circulation 2001; 103:2816-2821
- ** Simon C, Palmaz JC, Sprague EA. Influence of topography on endothelialization of stents: clues for new designes. J Lon Term Eff Med Implants. 2000;10:143-151

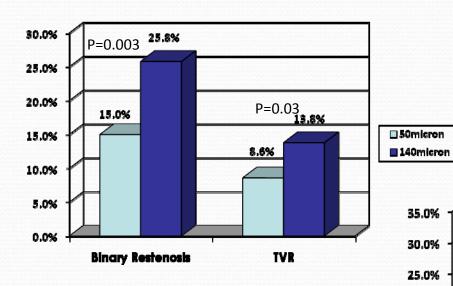






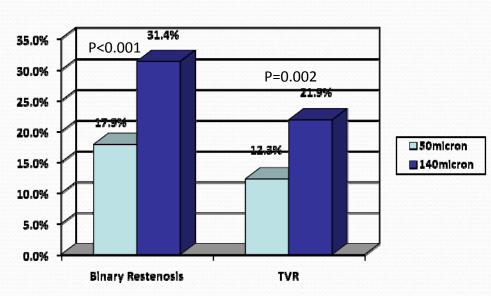


Thin is In!



ISAR-STEREO Trial. Circulation 2001;103:2816-2821

ISAR-STEREO 2 Trial. JACC 2003;41:1283-8





Mitsu – Technology Approach

Features

An "ultra-thin" stent.

Hybrid stent design = optimal geometry.

New sirolimus analogue with preferred dosing and drug release kinetics.

Polymer - free drug delivery.

Benefits

Lowest possible vessel wall injury (↓ inflammation)

Superior deliverability and conformability ("glove-like" fit and apposition)

Improved healing = less stent thrombosis

Lowest possible restenosis

Early discontinuation of DAPT



Strut

thickness

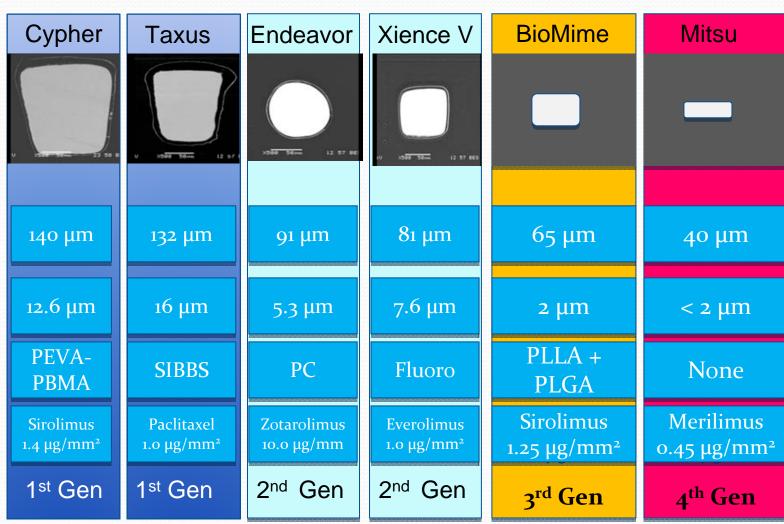
Coating

thickness

Polymer

Drug

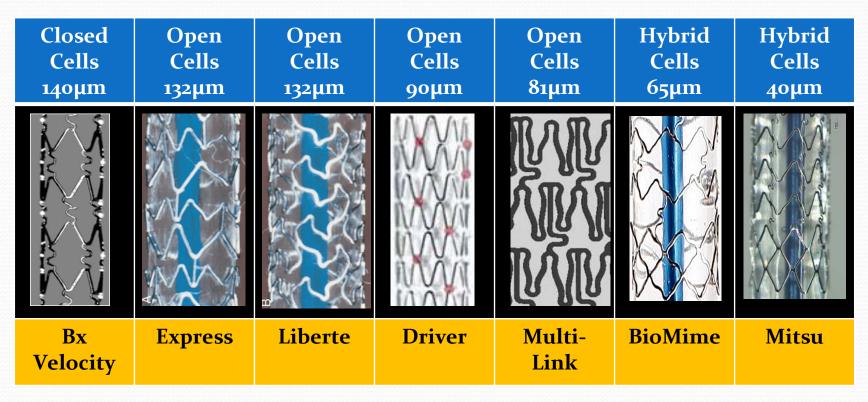
Moving towards biomimicry



3.0 mm diameter stents, 500X magnification

2000

Stent design makes a difference!



The "hybrid" design coupled with strut width variability eliminates the need for high strut thicknesses as required in earlier stent technologies

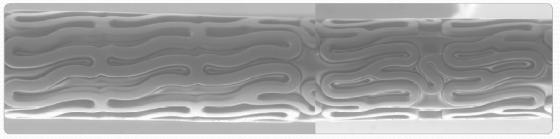
Closed cells Open cells

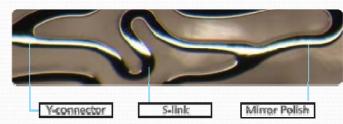


BioMime Stent Architecture

- Cobalt chromium (L605) platform with 65µm strut thickness.
- Hybrid cell design comprising of an intelligent mix of open and close cells resulting in excellent radial strength with a high flexibility.
- Unique strut width variability that ensure a <3% recoil and 0.29% foreshortening
- Special electro-polishing technique eliminates surface nickel oxides

SEM image of crimped BioMime SES at 50x

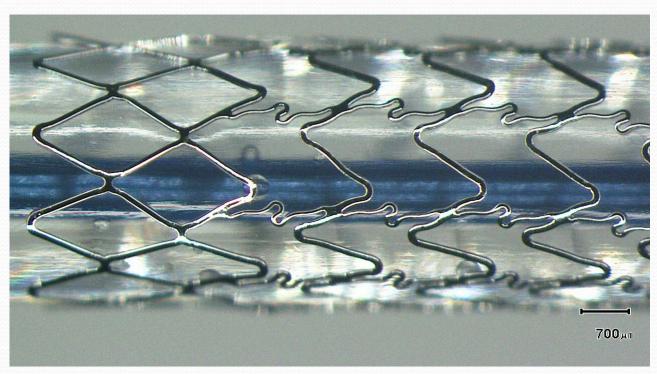




Closed cell at edges Open cell in mid - segment Hybrid design



Mitsu – Cell Architecture





Close cells at the edges

Open cells at the middle



Mitsu – Stent Features

Material of construction	Cobalt Chromium L605			
Strut thickness	40μm / 0.0016"			
Strut width	Variable 50μm - 100μm			
Dimensions	63 sizes - Ø 2.25 – 4.5mm / \$\ell 8 - 40mm\$			
Stent design	Hybrid – open cells in the middle and close at the edges			
Radial strength	High 1.1 <u>+</u> 0.10 ATM			
Recoil	Low 3.26%			
Foreshortening	Low 0.26%			
Metal to artery ratio	16% - 18%			
Pushability / Trackability	Excellent			
Dog boning effect	Uniform expansion			
Crossing profile crimped stent (3.0mm)	Low 0.96mm / 0.037"			

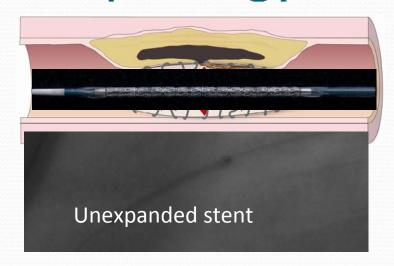


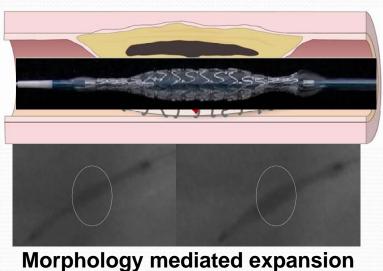
Low injury design

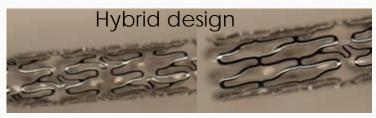
- Conventional edge-flaring stent designs allow the stent to dog-bone during deployment.
- This dog-boning coupled with balloon overhang may cause edge injury.
- BioMime has struts with design variability which results in morphology mediated expansion[™], having a propensity to minimize stent edge injury.



Morphology Mediated Expansion







Open cells in mid segment Close cells at edges

Propensity to minimize edge-injury

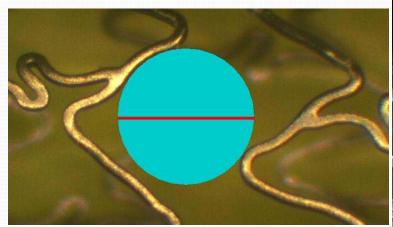


Note the narrow balloon shoulders which assist in minimizing balloon related vessel injury

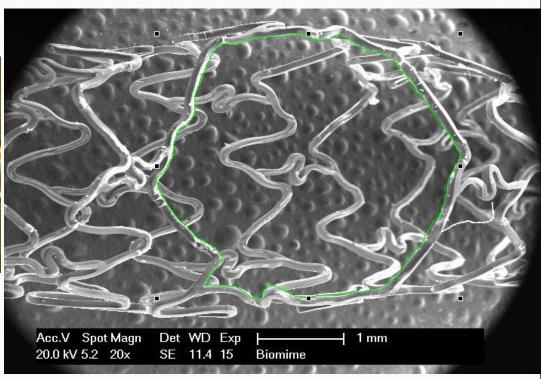




Excellent Side Branch Access



The area of the largest circle circumscribable in the cell of the stent expanded to the nominal diameter: $T_c = 0.71 \text{ mm}^2$



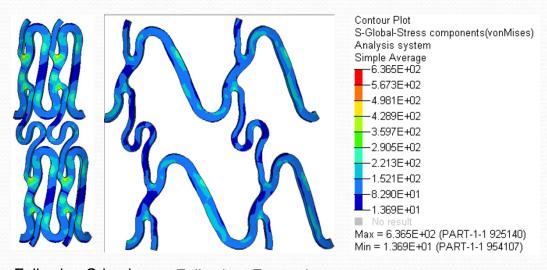
The expanded BIOMIME 3.0 x 16 mm stent after side branch expansion

Expanded cell perimeter that ensures side branch access: K_{SBA} = 11.29 mm Expanded cell area that ensures side branch access: T_{SBA} = 8.00 mm²

Data on file with Meril Life Sciences.

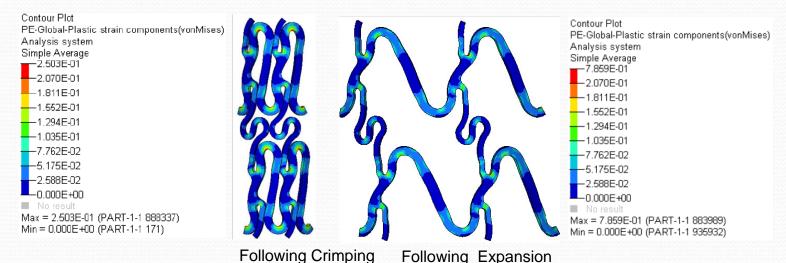


FEA Analysis



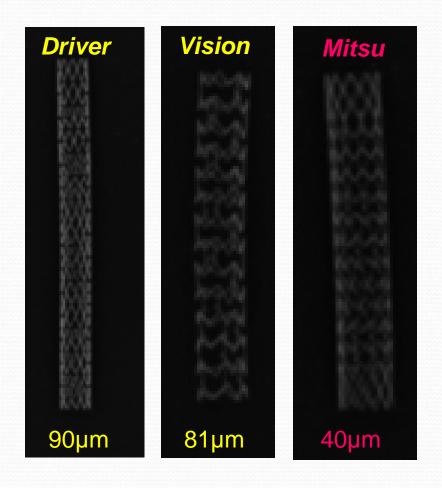
Following Crimping

Following Expansion





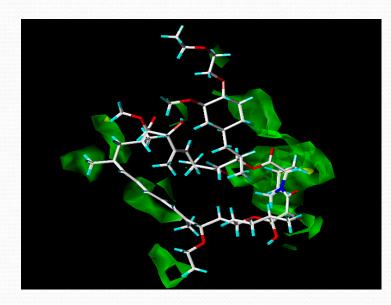
Mitsu - Relative Radio-opacity



Equivalent radio-opacity due to stent design



Merilimus



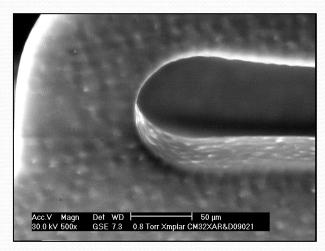
fkBP-12 receptor site adaptation by Merilimus molecule

- Merilimus is a Meril Life Sciences invention.
- Heterogeneous 5 member ring on the parent limus molecule.
- Better toxicological profile than Sirolimus and a wider therapeutic window (more lipophilic).
- Low drug dosing of 0.4µg/mm² possible to get optimal antiproliferative effect.

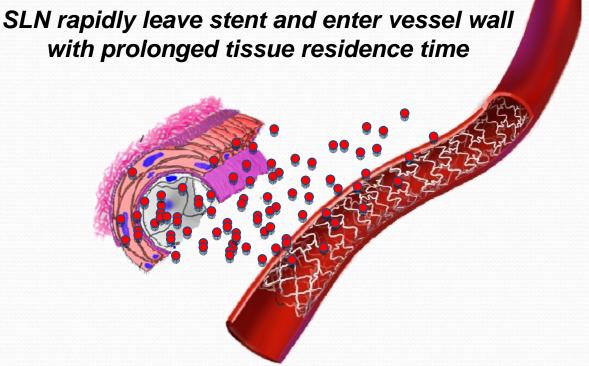


Nanotechnology

Unique Formulation - Solid lipid nano-spheres (SLN) consisting of Merilimus + Lipid (<500 nm)



SEM Image of Stent struts coated with nano-formulation





Nanotech for Drug Delivery

Potential Benefits of Solid-Lipid Nanoparticles

- Control and maintain in-tissue drug release
- Improved PK stability
- Enhanced cellular uptake
- Feasibility of carrying both lipophilic and hydrophilic drugs
- Lipids are biodegradable (excellent biocompatibility)
- Potential for lowering doses
- Potential to target different vascular layers by using differential NP size



Avg. Particle Size & Size Distribution

Z-Average (nm): 165.3763 Standard Deviation: 0

Variance: 0

%Std Deviation: 0

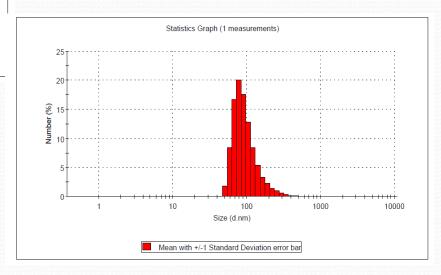
Derived Count Rate (kcps): 520810.981471...

Standard Deviation: 0
%Std Deviation: 0

Variance: 0

1	Size	Mean	Std Dev	Size	Mean	Std Dev	ſ	Size	Mean	Std Dev	Size	Mean	Std Dev
	d.nm	Number %		d.nm	Number %	Number %		d.nm	Number %	Number %	d.nm	Number %	Number %
ı	0.4000	0.0		5.615	0.0		ľ	78.82	20.0		1106	0.0	
	0.4632	0.0		6.503	0.0			91.28	17.5		1281	0.0	
	0.5365	0.0		7.531	0.0			105.7	12.8		1484	0.0	
	0.6213	0.0		8.721	0.0			122.4	8.5		1718	0.0	
	0.7195	0.0		10.10	0.0			141.8	5.3		1990	0.0	
	0.8332	0.0		11.70	0.0			164.2	3.4		2305	0.0	
	0.9649	0.0		13.54	0.0			190.1	2.2		2669	0.0	
	1.117	0.0		15.69	0.0			220.2	1.4		3091	0.0	
	1.294	0.0		18.17	0.0			255.0	0.9		3580	0.0	
	1.499	0.0		21.04	0.0			295.3	0.5		4145	0.0	
	1.736	0.0		24.36	0.0			342.0	0.3		4801	0.0	
	2.010	0.0		28.21	0.0			396.1	0.2		5560	0.0	
	2.328	0.0		32.67	0.0			458.7	0.1		6439	0.0	
	2.696	0.0		37.84	0.0			531.2	0.0		7456	0.0	
	3.122	0.0		43.82	0.0			615.1	0.0		8635	0.0	
	3.615	0.0		50.75	1.8			712.4	0.0		1.000e4	0.0	
	4.187	0.0		58.77	8.4			825.0	0.0				
	4.849	0.0		68.06	16.7		Į	955.4	0.0				

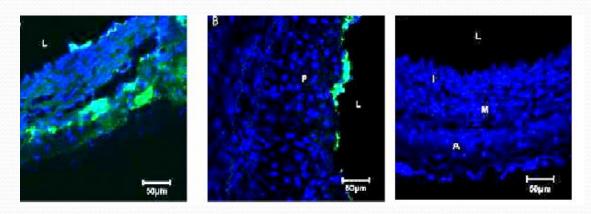
Size distribution of Drug-Lipid Nanoparticles between 50nm and 500nm (80% ~127nm) Average Particle Size (Z-Average): 165.4 nm





Nanotech for Drug Delivery

- Atherosclerotic plaque can be barrier to micro-particle vessel wall penetration; particle sizes < 300 nm are well suited for intra luminal drug delivery¹
- < 110 nm Particles will reach up to adventitia layer in considerable amount¹



Confocal images shows distribution of different size NP's in different arterial layers

1. Biodegradable paclitaxel loaded nanoparticles & stent coatings as local delivery systems for the prevention of restenosis. Dissertation. Dr. Thomas Kissel. Inst. for pharmaceutical technologie and biopharmacie, Marburg. 2004



Nanoparticle Stability – Zeta potential

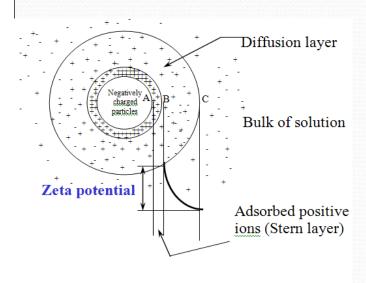


Fig. 1 Double Layer

Table 1: Stability of suspensions with relation to Zeta Potential (Riddick, 1968)

Stability Characteristics	Avg. Zeta Potential in mV
Maximum agglomeration and precipitation	0 to +3
Range of strong agglomeration and precipitation	+5 to -5
Threshold of agglomeration	-10 to -15
Threshold of delicate dispersion	-16 to -30
Moderate stability	-31 to −40
Fairly good stability	-41 to -60
Very good stability	-61 to -80
Extremely good stability	-81 to -100



The Zeta potential value (-53.9 mV) indicates Good Stability of Drug-lipid nano particles in suspension.

Zeta potential is the charge that develops at the interface between a solid Nanoparticles surface and aqueous medium. This potential, which is measured in MilliVolts, these are the dissociation of ionogenic groups in the particle surface and the differential adsorption of solution ions into the surface region.

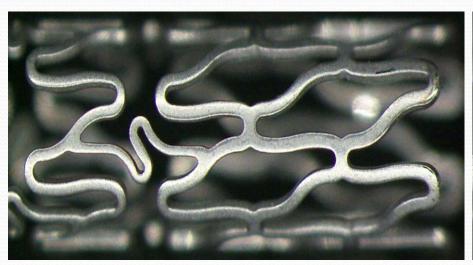


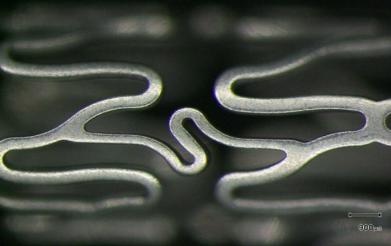
Mitsu – The formulation

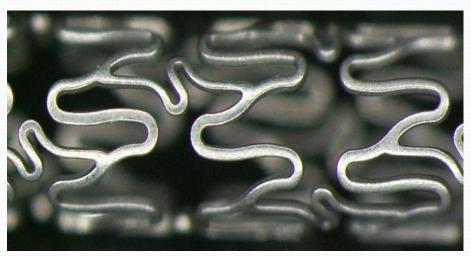
- Nanotechnology based coating.
- Designed for coating uniformity and lower drug dosage.
- Controlled and reproducible drug release kinetics.
- Rapid release of drug into tissue with "in-tissue" drug depot or reservoir effect.
- Renders the stent "coating-free" within a short time
 - Rapid tissue absorption (SLN has high tissue diffusion coefficient)
 - Formulation ensures drug availability for 1 month

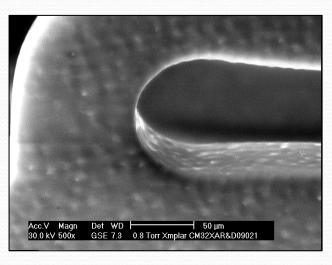


Optical Microscopic Images (Coating)









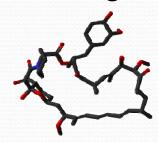


Mitsu - Summary

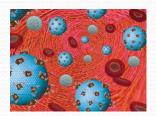
Stent System



Drug



Drug Delivery



- 40 μm thin stent
- Cobalt Chromium L605
- Hybrid stent design
- Variable strut width
- Tapered balloon shoulders

- Merilimus new limus analogue
- Cytostatic, anti-inflammatoryand lipophilic
 - Wide therapeutic window

- Novel SLN polymer-free formulation
- Low drug for same effect
- Fast release kinetics
- Completely biocompatible and anti-inflammatory

A unique differentiated new DES!